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Formulation and Evaluation of Rita B* and Sustained Release Matrix Tablets of Nifedipine

Abstract

Conventional drug delivery system for treating the angina and hypertension are not much effective as the drug do not reach the site of action in appropriate amounts. Thus potent and guarded therapy of this angina and hypertension disorder using specific drug delivery system is a challenging task to the pharmaceutical professionals. Most oftenly used method of regulating the drug release is to include it in a matrix system because of their pliability, hydrophilic polymer matrices are widely used in oral controlled drug delivery to obtain a desirable drug release pattern, methodical, and broad regulatory compliance. Formulation of Nifedipine sustained release matrix tablet was prepared by the polymers blend with to get desirable drug release profile. Evaluation parameters of formulated tablets were hardness, friability, thickness, drug content uniformity weight variation, and the in vitro drug release rate pattern. Formulation prepared with HPMC K100M showed 97% of drug release at 24 hrs and with Eudragit indicates 99% of drug release at 20 hrs release of Nifedipine drug.

Keywords: Nifedipine; Eudragit; HPMC; Suatained release; Martix tablet

Suresh V

Department of Pharmaceutics, G. Pulla Reddy College of Pharmacy, Osmania University, India

Corresponding author: Rita B

badigeru.rita@gmail.com

Department of Pharmaceutics, G. Pulla Reddy college of Pharmacy, Osmania University, Hyderabad, India

Tel: +919642701807

Introduction

Sustained release dosage form is a modified dosage form that prolongs the therapeutic activity of the drug. Sustained release products provide an immediate release of drug that promptly produces the desired therapeutic effect which is followed by gradual release of additional amounts of drug to maintain this effect over a predetermined period of time. sustained release products often times eliminates the need for night dosing, which benefits not only the patients but the care given as well because of the sustained plasma drug levels [1,2].

The basic rationale of a sustained drug delivery system is to optimize the Pharmacodynamics and Pharmacokinetic properties of a drug in such a way that its utility is maximized through reduction in side effects and cure or control of condition in the shortest possible time by using smallest amount of drug which is administered by the most effective route. Oral route has been the most popular and widely used for sustained delivery of drugs because of convenience and ease of administration, greater flexibility in dosage form design, ease of production and low cost.

Most conventional oral drug products, such as tablets and capsules, are formulated to release the active drug immediately after oral administration, to obtain fast and complete systemic drug absorption. Such immediaterelease products results in rapid drug absorption and onset of action. Plasma drug concentration reduces according to the drug's pharmacokinetic profile after absorption of the drug from the dosage form is absolutely complete. Plasma drug concentrations fall below the minimum effective plasma concentration (MEC), resulting in failure of therapeutic efficacy. Before this point is attained, the other dose is usually given if a sustained therapeutic outcome is desired. The other way of administering dose is to utilize a dosage form that will provide sustained release of drug by maintaining the plasma drug concentrations [3,4].

Materials and Methods

Nifedipine, HPMC-E5, HPMCK100, Eudragit, Magnesium Stearate Lactose, Micro crystalline Cellulose

Wet granulation technique

Steps Involved In Wet Granulation Method for Preparation of Tablets

- 1. Mixing of the drug(s) and excipients
- 2. Preparation of binder solution
- 3. Mixing of binder solution with powder mixture to form wet mass
- 4. Coarse screening of wet mass using a suitable sieve (6-12 screens)
- 5. Drying of moist granules

 Table 1 Nifedipine formulation.

| INGREDIENTS | F1 | F2 | F3 | F4 | F5 | F6 | F7 | F8 | F9 |
|-----------------|-----|----|----|-----|----|----|-----|----|----|
| NIFEDIPINE(mg) | 30 | 30 | 30 | 30 | 30 | 30 | 30 | 30 | 30 |
| HPMCE5(mg) | 10 | 20 | 30 | - | - | - | - | - | - |
| HPMCK100(mg) | - | - | - | 10 | 20 | 30 | - | - | - |
| EUDRAGIT(mg) | - | - | - | - | - | - | 10 | 20 | 30 |
| Mg.STEARATE(mg) | 2 | 2 | 2 | 2 | 2 | 2 | 2 | 2 | 2 |
| LACTOSE(mg) | 50 | 50 | 50 | 50 | 50 | 50 | 50 | 50 | 50 |
| MCC(mg) | 108 | 98 | 88 | 108 | 98 | 88 | 108 | 98 | 88 |

Table 2 API characterisation.

| s.no | API Characterisation | results |
|------|----------------------|--|
| 1 | Physical Appearance | Nifedipine is a yellow crystalline substance |
| 2 | Melting point | 172-174°C |
| 3 | Solubility | It is freely soluble in ethanol |

Table 3 Pre compression parameters.

6. Screening of dry granules through a suitable sieve (14-20 screen)

7. Mixing of screened granules with glidant and lubricant (Table 1).

Results

API characterization

The flow properties of the prepared blend were studied with given IP limits. The hausner's ratio [5] was found to be excellent and passable in the range of 1.09-1.33 and compressibility index in range of 8.6%-25% **(Tables 2 and 3)**.

Post compression parameters

The hardness was constantly maintained between 4-6 kg/cm² for all formulations during compression. Shows the friability values all the formulations [6]. The results indicated that the % friability was between the ranges. The low values of friability indicate that tablets were mechanically hard enough. The drug content of tablets ranged between 97 and 100. The weight variation of all formulations was in the range of 197.6 \pm 1.15 to 203.8 \pm 1.12 **(Table 4)**.

In vitro dissolution studies

The dissolution conditions used for studying the drug release from Dosage form:

Apparatus: USP apparatus II (Paddle),

Agitation speed (rpm): 100 rpm,

Medium: 6.8 pH phosphate buffer

Volume: 900 ml

| FORMULA | ANGLE OF REPOSE | BULK DENSITY (gm/ml) | TAPPED DENSITY (gm/ ml) | CARR'S INDEX % | HAUSNER'S RATIO |
|---------|-----------------|----------------------|----------------------------|----------------|-----------------|
| F1 | 26.6 ± 0.2 | 0.555 ± 0.1 | 0.714 ± 0.1 | 22.22 | 1.285 |
| F2 | 26.0 ± 0.3 | 0.384 ± 0.4 | 0.434 ± 0.3 | 11.53 | 1.130 |
| F3 | 26.7 ± 0.4 | 0.416 ± 0.2 | 0.476 ± 0.3 | 12.50 | 1.142 |
| F4 | 25.1 ± 0.1 | 0.476 ± 0.3 | 0.526 ± 0.2 | 9.52 | 1.105 |
| F5 | 28.3 ± 0.4 | 0.625 ± 0.1 | 0.833 ± 0.1 | 25.00 | 1.333 |
| F6 | 24.4 ± 0.4 | 0.521 ± 0.3 | 0.631 ± 0.3 | 17.39 | 1.121 |
| F7 | 27.1 ± 0.1 | 0.588 ± 0.3 | 0.666 ± 0.4 | 11.76 | 1.333 |
| F8 | 25.2 ± 0.1 | 0.277 ± 0.2 | 0.312 ± 0.2 | 11.11 | 1.133 |
| F9 | 23.2 ± 0.2 | 0.434 ± 0.2 | 0.476 ± 0.3 | 8.695 | 1.095 |

Table 4 Post compression parameters.

| FORMULA | THICKNESS (mm) | HARDNESS (Kg/cm ²) | %FRIABILITY (w/w) | WEIGHT VARIATION (mg) | DRUG CONTENT (%) |
|---------|----------------|--------------------------------|-------------------|--------------------------|------------------|
| F1 | 3.2 ± 0.05 | 4.0 ± 0.1 | 0.24 ± 0.03 | 201.8 ± 1.02 | 99.47 ± 0.3 |
| F2 | 3.1 ± 0.02 | 5.5 ± 0.1 | 0.07 ± 0.02 | 203.8 ± 1.12 | 98.89 ± 0.5 |
| F3 | 3.3 ± 0.07 | 5.0 ± 0.4 | 0.19 ± 0.03 | 202.4 ± 1.02 | 98.35 ± 0.9 |
| F4 | 3.2 ± 0.03 | 4.5 ± 0.2 | 0.07 ± 0.01 | 202.1 ± 1.15 | 97.12 ± 0.5 |
| F5 | 3.2 ± 0.04 | 5.3 ± 0.1 | 0.16 ± 0.04 | 199.1 ± 1.13 | 97.56 ± 0.6 |
| F6 | 3.1 ± 0.02 | 5.4 ± 0.3 | 0.07 ± 0.03 | 198.1 ± 1.15 | 98.35 ± 0.3 |
| F7 | 3.3 ± 0.02 | 5.5 ± 0.4 | 0.07 ± 0.01 | 198.6 ± 1.15 | 98.40 ± 0.4 |
| F8 | 3.2 ± 0.05 | 5.4 ± 0.2 | 0.24 ± 0.02 | 197.6 ± 1.15 | 97.84 ± 0.3 |
| F9 | 3.2 ± 0.03 | 5.7 ± 0.2 | 0.04 ± 0.01 | 201.6 ± 1.15 | 99.64 ± 0.1 |

Temperature: 37.0 ± 0.5°C

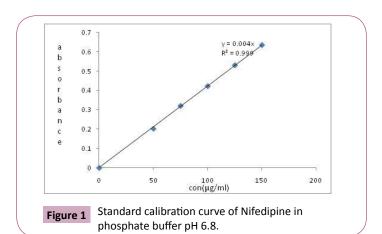
Time: 1, 4, 8, 12, 16 and 20 hrs.

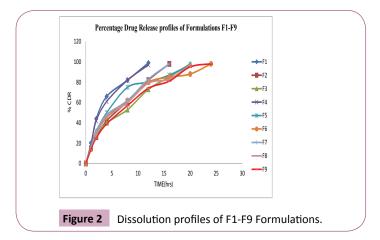
Wavelength: 238 nm

The samples were withdrawn at predetermined time points, and were analyzed spectrophotometrically at 238 nm(Figure 1). The prepared tablets were subjected to dissolution studies in order to know the amount of drug released and the results of percentage drug release are shown in **Table 5**. As the concentration of polymer increased, the drug release decreased [7]. In vitro drug release studies revealed that release of Nifedipine from different formulations varies with characteristics and composition of matrix forming polymers. The release rate increased with decreasing concentration of HPMC. These findings are in compliance with the ability of HPMC to form complex matrix network which leads to delay in release of drug from device. Eudragit is hydrophobic polymer which delays the drug release in F7 to F9.

Dissolution profile of formulations F1-F9

The Figure 2 shows the in vitro release profiles of Nefidipine [8] sustained release matrix tablets of formulations F1-F9. Effect of different polymers on the release profile of Nifedipine was studied. In formulations F1, F2, F3 different concentrations of HPMCE5 were used [9]. The release of the drug from the tablet was up to 20 hours only, so these polymers (with in this concentrations) not having the capacity to extend the release up to 24 hours **(Table 5).** In formulations F4, F5, F6 different





concentrations of HPMCK100 were used [10]. The release of the drug from the tablet was up to 24 hours these polymers (with in this concentrations) having the capacity to extend the release up to 24 hours. In formulations F7, F8, F9 different concentrations of Eudragit were used [11]. The release of the drug from the tablet was up to 24 hours these polymers (with in this concentrations) having the capacity to extend the release up to 24 hours.

Release kinetics and mechanism

To know the release mechanism and kinetics of Valsartan optimized formulations (F14) were attempted to fit into mathematical models and n, r^2 values for zero order [12], First order, Higuchi and Peppas models were represented in **Table 6**. The peppas model is widely used, when the release mechanism is not well known or more than one type of release could be involved. The semi-empirical equation (Peppas et al.,) [13] shown as equation:

Mt/M∞=ktⁿ

Where, Mt/M ∞ is fraction of drug released at time't', k represents a constant, and n is the diffusional exponent, which characterizes the type of release mechanism during the dissolution process (Tables 6 and 7). For non-fickian release, the value of n falls between 0.5 and 1.0; while in case of fickian diffusion, n=0.5; for zero-order release (case II transport), n=1; and for supercase II transport, n > 1

Stability studies

There was no significant change in physical and chemical properties of the tablets of formulation F-9 after 3 Months. Parameters quantified at various time intervals were shown in **Table 8**.

Conclusion

Nifedipine is used in angina. In the present work sustained release tablet was successfully formulated by using different polymers by wet granulation method. The drug-excipient interaction study was carried out using FTIR. In the drug-excipient interaction study, it was found that Nifedipine was having compatibility with all the excipients used in the formulation. Ingredients used are Eudragit, HPMC-E5 and HPMCK100, Lactose, Magnesium Stearate, and Microcrystalline Cellulose.

The optimized formula shows, Hardness – 5.7 kg cm^2 , Friability – 0.04, %CDR – 99.

From the *in vitro* dissolution analysis the following conclusions are drawn. Formulation batches with HPMC K100 and EUDRAGIT [14] showed better release than the HPMCE5. It was observed that by increasing the viscosity of polymer a retarding effect on the release from the polymer matrix [15,16]. From the dissolution profile modeling it was found that the optimized formulation F9 followed first order release kinetics and Koresmayer Peppas model [17]. Since n>0.5 non Fickian or anomalous diffusion behaviour is generally observed. When the stability results of best formulae was studied at 40°C AND 75% RH for 3

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months were compared with their initial results it was found that there was no significant difference in hardness, friability, drug content and drug release of optimized formulation.

| TIME (Hrs) | F1 %CDR | F2 %CDR | F3 %CDR | F4 %CDR | F5 %CDR | F6 %CDR | F7 %CDR | F8 %CDR | F9 %CDR |
|------------|--------------|--------------|--------------|--------------|--------------|--------------|--------------|--------------|--------------|
| 1 | 20.45 ± 0.51 | 15.0 ± 0.46 | 16.36 ± 0.31 | | 18.40 ± 0.35 | | 16.70 ± 0.15 | 15.20 ± 0.25 | 14.27 ± 0.12 |
| 2 | | | | | 32.04 ± 0.54 | | | | |
| 4 | 44.65 ± 0.23 | 26.59 ± 0.32 | 28.63 ± 0.26 | | | | | 28.63 ± 0.32 | 25.5 ± 0.31 |
| 8 | 66.13 ± 0.33 | 42.61 ± 0.62 | 40.22 ± 0.53 | 61.36 ± 0.32 | 50.93 ± 0.34 | 46.06 ± 0.25 | 48.06 ± 0.55 | 45.18 ± 0.63 | 39.36 ± 0.25 |
| | 82.5 ± 0.21 | 61.02 ± 0.22 | 53.86 ± 0.23 | 82.84 ± 0.25 | 75.22 ± 0.44 | 62.34 ± 0.65 | 62.04 ± 0.51 | 60.09 ± 0.34 | 57.04 ± 0.63 |
| 12 | 99.20 ± 0.36 | 82.84 ± 0.52 | 73.29 ± 0.65 | 97.84 ± 0.35 | 80.52 ± 0.42 | 80.02 ± 0.51 | 83.86 ± 0.15 | 76.43 ± 0.62 | 74.38 ± 0.32 |
| 16 | | 98.52 ± 0.24 | 85.56 ± 0.65 | | 87.84 ± 0.33 | 85.45 ± 0.23 | 98.18 ± 0.32 | 83.52 ± 0.52 | 81.11 ± 0.11 |
| 20 | | | 98.18 ± 0.21 | | 97.84 ± 0.31 | 88.29 ± 0.51 | | 97.84 ± 0.61 | 95.0 ± 0.21 |
| 24 | | | | | | 97.18 ± 0.23 | | | 99.20 ± 0.31 |

Table 5 Results of dissolution profile for F1-F9.

Table 6 kinetic modeling of F1-F9.

| Formulation code | Zero Order | First Order | Higuchi | Hixon Crowell | KoresmeyerPeppas | | |
|------------------|-------------------|-------------------|-------------------|-------------------|------------------|--------|--|
| code | (R ²) | (R ²) | (R ²) | (R ²) | R ² | n | |
| | | | | | | | |
| F1 | 0.873 | 0.9161 | 0.9785 | 0.9771 | 0.9345 | 0.607 | |
| | | | | | | | |
| F2 | 0.8856 | 0.9683 | 0.9872 | 0.9695 | 0.9967 | 0.664 | |
| | | | | | | | |
| F3 | 0.9565 | 0.8778 | 0.992 | 0.966 | 0.991 | 0.578 | |
| | | | | | | | |
| F4 | 0.8927 | 0.9689 | 0.9846 | 0.9902 | 0.9464 | 0.624 | |
| | | | | | | | |
| F5 | 0.8652 | 0.9526 | 0.9779 | 0.9689 | 0.9673 | 0.544 | |
| | | | | | | | |
| F6 | 0.8782 | 0.9292 | 0.9816 | 0.9711 | 0.957 | 0.571 | |
| | | | | | | | |
| F7 | 0.9442 | 0.8917 | 0.9906 | 0.9689 | 0.9802 | 0.5957 | |
| | | | | | | | |
| F8 | 0.9215 | 0.9211 | 0.9916 | 0.9747 | 0.9803 | 0.5957 | |
| | | | | | | | |
| F9 | 0.9313 | 0.9498 | 0.9827 | 0.9874 | 0.9887 | 0.4357 | |

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Table 7 kinetic model for optimized formula.

| S.NO | Time | log T | Square root of Time | %CR | %Drug remaining | log %CR | log% Drug retained | Cube root of %drug remaining |
|------|------|----------|------------------------|-------|--------------------|----------|-----------------------|------------------------------------|
| 1 | 0 | 0 | 0 | 0 | 100 | 0 | 2 | 4.641589 |
| 2 | 1 | 0 | 1 | 14.27 | 85.73 | 1.154424 | 1.933133 | 4.409381 |
| 3 | 2 | 0.30103 | 1.414214 | 25.5 | 74.5 | 1.40654 | 1.872156 | 4.207771 |
| 4 | 4 | 0.60206 | 2 | 39.36 | 60.64 | 1.595055 | 1.782759 | 3.928738 |
| 5 | 8 | 0.90309 | 2.828427 | 57.04 | 42.96 | 1.75618 | 1.633064 | 3.502311 |
| 6 | 12 | 1.079181 | 3.464102 | 74.38 | 25.62 | 1.871456 | 1.408579 | 2.947993 |
| 7 | 16 | 1.20412 | 4 | 81.11 | 18.89 | 1.909074 | 1.276232 | 2.663242 |
| 8 | 20 | 1.30103 | 4.472136 | 95.03 | 4.97 | 1.977861 | 0.696356 | 1.706549 |
| 9 | 24 | 1.380211 | 4.898979 | 99.2 | 1.8 | 1.992111 | 0.255273 | 1.21644 |

Table 8 Stability studies.

| Formulation Code | Parameters | Initial | 1 st Month | 2 nd Month | 3 rd Month |
|------------------|-------------|------------------|-----------------------|-----------------------|-----------------------|
| F9 | 25°C/60%RH | 25°C/60%RH 99.18 | | 99.17 | 99.15 |
| | 30°C/75% RH | 99.20 | 99.18 | 99.17 | 99.15 |
| | 40°C/75% RH | | 99.18 | 99.17 | 99.15 |

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