



# Formulation development and evaluation of long acting ophthalmic in-situ gelling system of Dorzolamide Hydrochloride

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## Abstract:

This research paper describes the objective of the present study to formulate ophthalmic mucoadhesive *in situ* gelling system of Dorzolamide Hydrochloride using two different polymers namely Poly Acrylic Acid and Xanthan Gum, individually and in combinations. Cellulose (HPMC) was used as viscosity enhancing agent. The developed formulations were subjected to several evaluation parameters including physico-chemical properties, compatibility, *in-vitro* drug release, microbiological, *ex-vivo* and stability testing and compared with marketed formulation wherever possible. All formulations were found to be milky with pH between 6.0 to 6.5 for sols and nearly neutral for gels. All formulations showed instantaneous gelling with translucent gel matrix which retained its integrity for extended period of time. The viscosity of best formulation (F4) was found to be 20 cps. The drug was compatible with both the polymers and the viscoliser in both solid as well as liquid states. *In-vitro* drug release studies showed that all the formulations released drug over a period of 12 hours with formulation F4 (0.2% w/v Xanthan Gum) showing the highest drug release of 90.84% of Dorzolamide Hydrochloride. All the formulations showed zero order drug release with the release mechanism being diffusion along with erosion of gel matrix for all formulations. Further the drug release from all the formulation was observed to be non-fickian. The best batch showed *ex-vivo* drug release through goat's cornea for 9 hours with the release kinetics being similar to those seen with *in-vitro* drug release. All the formulations were found to be sterile.

**Keywords:** Mucoadhesive, Dorzolamide Hydrochloride, PolyAcrylic Acid, Xanthan Gum, Non-fickian.

## Introduction

Eye is the most interesting organ due to its drug disposition characteristics. The poor accessibility of a number of ocular regions to systemic circulation makes local delivery via topical administration the preferred route for the treatment of ocular diseases. Typical conditions that require ocular administration include corneal disorders (i.e. glaucoma) and eye infections (i.e. conjunctivitis)<sup>[1]</sup> Ophthalmic drug delivery is one of the most interesting and challenging endeavours facing the pharmaceutical scientist. The biological barriers involved for ocular delivery are the permeability barriers posed by cornea and other regions, as well as the tear washout and blinking reflexes designed to remove foreign substances from the eye. A significant challenge to the formulator is to circumvent (bypass) the protective

barriers of the eye without causing permanent tissue damage.<sup>[2]</sup> A significant challenge to the formulator is to circumvent (bypass) the protective barriers of the eye without causing permanent tissue damage.<sup>[2]</sup> Furthermore the ocular region is very sensitive and cannot withstand high local concentrations of drugs and vehicles without irritation. Because of these limitations, designing formulations and delivery systems for topically applied ophthalmic drugs is challenging. It requires thorough understanding of physiological basis of the protective mechanism designed by the eye which allows only 1- 10% of topically applied dose to be absorbed locally.<sup>[1]</sup>

Development of newer, more sensitive diagnostic techniques and novel therapeutic agents continue to provide ocular delivery systems with high therapeutic efficacy. Conventional ophthalmic formulations like solution, suspension,

and ointment have many disadvantages which result into poor bioavailability of drug in the ocular cavity. The specific aim of designing a therapeutic system is to achieve an optimal concentration of a drug at the active site for the appropriate duration. Ocular disposition and elimination of a therapeutic agent is dependent upon its physicochemical properties as well as the relevant ocular anatomy and physiology. A successful design of a drug delivery system, therefore, requires an integrated knowledge of the drug molecule and the constraints offered by the ocular route of administration [2]

The various approaches that have been attempted to increase the bioavailability and the duration of the therapeutic action of ocular drugs can be divided into two categories. The first one is based on the use of sustained drug delivery systems, which provide the controlled and continuous delivery of ophthalmic drugs. The second involves maximizing corneal drug absorption and minimizing precorneal drug loss.[2] Ideal ophthalmic drug delivery system must be able to sustain the drug release and to remain in the vicinity of front of the eye for prolong period of time. Such systems should be more hydrophobic, minimize interference with blinking and exhibit pseudoplastic behaviour. A better approach of ocular product behaviour coupled with formulation optimization can lead the way to development of newer ocular drug delivery systems.[3]

## MATERIALS AND METHODS

Dorzolamide hydrochloride was obtained from Cipla Ltd., Verna Goa. Xanthan Gum was obtained from Lucid Colloids Ltd., Mumbai. Carbopol 971 P from Lubrizol, Mumbai. HPMC

K4M of pharma grade was procured by Colorcon Asia, Verna-Goa. Benzalkonium Chloride from Centaur Pharmaceuticals Karaswada Mapusa. Mannitol, Disodium edentate, Potassium dihydrogen ortho- phosphate, Sodium hydroxide all were laboratory reagent obtained from lobachemie. FTIR Spectrophotometer of Prestige-21FTIR Shimadzu was used. UV Spectrophotometer of Perkin Elmer Lambda 25 was used.

Selection of Vehicle Solubility of Dorzolamide hydrochloride was tested in distilled water and a series of Phosphate Buffers of different pH. Phosphate buffer pH 6.8 was selected as vehicle as it formed sols having pH value close to pH 6 as using distilled water resulted acidic solutions having pH value less than 5.

Determination of *In situ* gelling concentration was done in Aqueous solutions of both the polymers decided to be used in the formulations, i.e. Xanthan Gum and Carbopol 971P were prepared in concentrations ranging from 0.1% to 1.0% (with and without 0.2% HPMC) and tested for gelling capacity. Gelling capacity was determined by placing a drop of the system in a vial containing 2 ml of artificial tear fluid freshly prepared and equilibrated to 37<sup>o</sup> C and visually assessing the gel formation and noting the time for gelation and the time taken for the gel form to dissolve.

In both the cases, the minimum concentrations at which the respective polymers showed gelling were noted. The results are shown in the Table No.1

Polymer*	Minimum Concentration Showing Gelling In STF (%W/V)	
	WITHOUT HPMC	WITH HPMC
Xanthan Gum	0.35	0.2
Carbopol 971P	0.5	0.3

\* Polymers were in combination with HPMC (0.4% w/v)

**Table 1:** Determination of polymer concentration

## COMPOSITION OF FORMULATION

INGREDIENTS	F1	F2	F3	F4	F5	F6	F7
DORZOLAMIDE HYDROCHLORIDE	2	2	2	2	2	2	2
CARBOPOL 971P	0.3	0.4	0.5	---	---	---	0.2
XANTHAN GUM	---	---	---	0.2	0.25	0.3	0.1
HPMC K 4M	0.4	0.4	0.4	0.4	0.4	0.4	0.4
DISODIUM EDETATE	0.1	0.1	0.1	0.1	0.1	0.1	0.1
BENZALKONIUM CHLORIDE	0.01	0.01	0.01	0.01	0.01	0.01	0.01
MANNITOL	5	5	5	5	5	5	5
AQUEOUS BUFFER BASE	q.s	q.s	q.s	q.s	q.s	q.s	q.s

**Table 2:** Composition of Formulations (all the quantities are in %w/v)

Methodology adopted in which Polymer solution was prepared by soaking HPMC K4M and the polymer in 50 ml of phosphate buffer pH 6.8 in a beaker. Dorzolamide hydrochloride was dissolved in another portion of phosphate buffer. Benzalkonium chloride (BKC), edetate disodium (EDTA) and mannitol were then added to the above drug solution. The drug solution was added to the polymer solution with stirring taking precaution not to incorporate air bubbles. The final solution was then transferred to a 100 ml volumetric flask and the volume was made up with Phosphate buffer.

Estimation of dorazamide hydrochloride spectrophotometric method based on the measurement of absorbance at 253nm in solvent phosphate buffer pH 7.4 was used to estimate Dorzolamide Hydrochloride.

A) Preparation of Simulated Tear Fluid- Phosphate buffer pH 7.4

The buffer was prepared by mixing 50 ml of 0.2M Monobasic Potassium di hydrogen Ortho Phosphate with 39.1 ml of 0.2M Sodium Hydroxide and diluting it with distilled water to produce 200 ml.

B) Standard calibration curve of Dorzolamide Hydrochloride

Accurately weighed 10mg of Dorzolamide hydrochloride was dissolved in 100 ml phosphate buffer pH 7.4 to get a stock solution of 100 µg/ml.

From this stock solution aliquots of 3, 6, 9, 12, 15, 18, 21 and 24ml were withdrawn and further diluted to 100ml with buffer to obtain a concentrations range of 3 to 24 µg/ml.

The absorbance of the resulting solutions was measured at 253nm on a UV spectrophotometer using phosphate buffer pH 7.4 as blank. The standard curve was obtained by plotting a graph of absorbance v/s concentration (µg/ml). From the standard curve, the amount of Dorzolamide hydrochloride in the formulations was estimated.

Aqueous solutions of Carbopol 971P and Xanthan gum coupled with added viscolizers are attractive in-situ gel forming systems, promising controlled ocular drug delivery of Dorzolamide Hydrochloride. All the systems exhibited zero order kinetics suggesting drug release in a controlled manner and release profile was diffusion associated with erosion of the polymer. Devised formulations were found to be effective in vitro and ex vivo in management of related ocular pathological conditions.

Clarity is one of the important characteristic features of ophthalmic preparations.

pH is one of the most important parameter involved in the ophthalmic preparations.

The sols were further converted to gels using phosphate buffer pH 7.4 and the physical appearance of the gel was taken note off. pH is

one of the most important parameter involved in the ophthalmic formulation.

Measurement of pH was carried out for sols and the gels (obtained by neutralizing sols to gels with phosphate buffer pH 7.4) at room temperature with the help of a pH meter. The measurement of the time taken to form the gel and the extent of gellation was determined. The test was carried out in test tubes wherein the formulations were mixed with Simulated Tear Fluid (maintained at 37°C) in the proportion 25:7. The proportion is so chosen because the application volume of eye drops is usually 25 µl and the volume of tear fluid present is 7 µl. Also the time for which the formed gel retains its integrity was noted. Isotonicity is an important characteristic of ophthalmics. Formulation was mixed with few drops of blood and observed under microscope at 45X magnification and compared with standard marketed ophthalmic formulation containing dorzolamide.

FT-IR spectra of the individual drug and the drug polymer mixtures were taken using FTIR-IR (Prestige-21FTIR Shimadzu Sr. no. A21004401461) and the spectra were run from 400 to 2000 cm<sup>-1</sup> to rule out any possible incompatibilities in solid state. Calorimetric characterization of Dorzolamide hydrochloride alone and in combination with Carbopol, xanthan and HPMC K4M were carried out using a DSC 823e instrument (Mettler Toledo). Nitrogen was used as the purging gas at a rate of 10 ml/min. All experiments were performed using non-hermetic aluminium pans, into which samples were accurately weighed, and then simply covered with a lid. Culture media chosen must necessarily support growth of different microorganisms viz bacteria, moulds and yeasts. Therefore Soyabean Casein Digest Media (SCDM) as fungal media

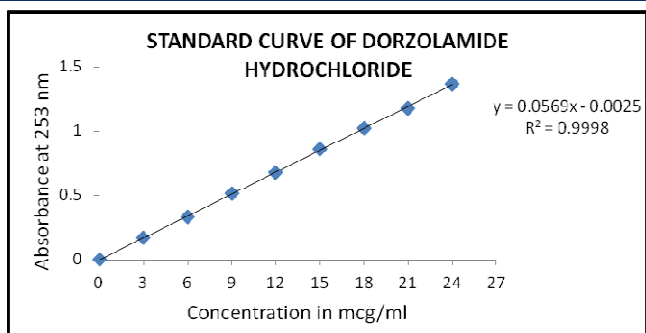
and Fluid Thioglycollate Media (FTG) as bacterial media, were used in a sterile condition after autoclaving at 121°C for 20 minutes at 15 psi. Ex vivo was done using goat skin using the permeability studies.

## RESULTS AND DISCUSSIONS

All the seven formulations were prepared and packed in 10 ml amber colored vials and sealed. Turbidity was noticed in the formulations, immediately after sterilization, which disappeared after cooling. The turbidity can be assigned to the precipitation of HPMC at high temperatures due to thermo-reversible gelation, which then disappeared after cooling. The Standard curve of Dorzolamide hydrochloride was recorded. Calibration table for the spectrophotometric determination of Dorzolamide hydrochloride is as given below which gives the absorbance values of Dorzolamide hydrochloride standard solutions containing 2-10 µg/ml of drug in phosphate buffer pH 7.4. Figure 1 shows the standard calibration curve with slope 0.0569 and regression coefficient 0.9998. The calculations of Drug Content Uniformity, *In vitro* drug release studies and stability studies are based on this calibration curve.

Concentration in µg/ml	Absorbance at 253nm
3	0.1694
6	0.3306
9	0.5134
12	0.6756
15	0.8574
18	1.0249
21	1.1798
24	1.3682

**Table 3:** Concentration vs Absorbance



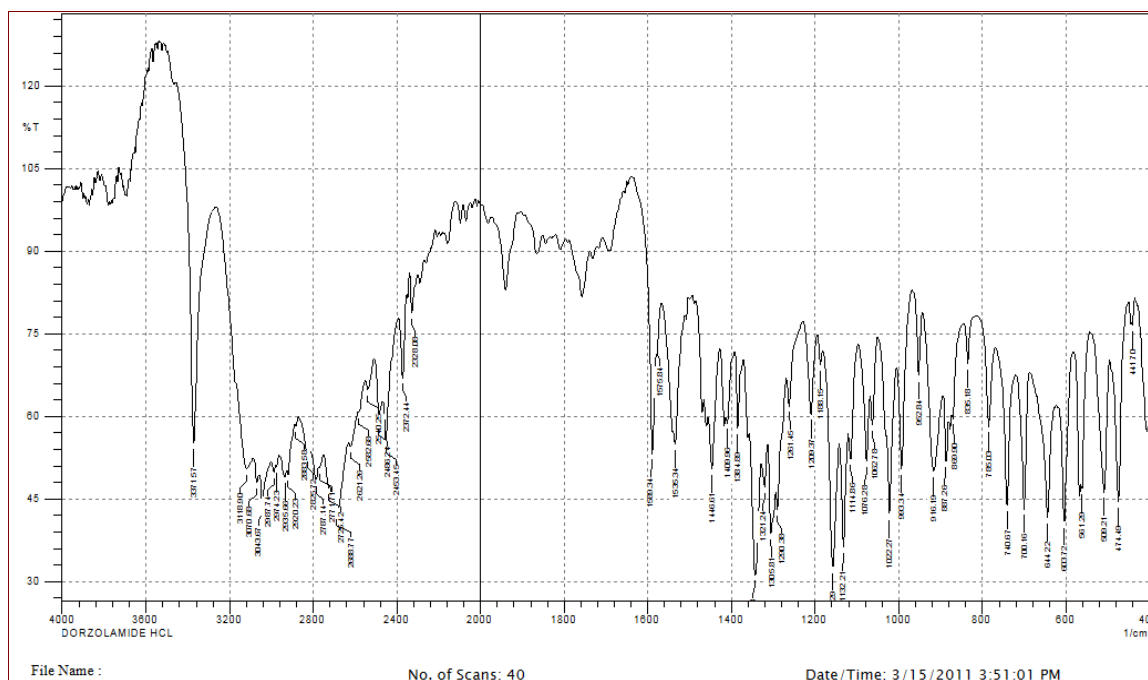
**Fig 1:** Standard calibration curve of Dorzolamide hydrochloride

Graph of concentration vs absorbance in which a linear increase in absorbance is achieved with increase in concentration. Both quantities are directly proportional.

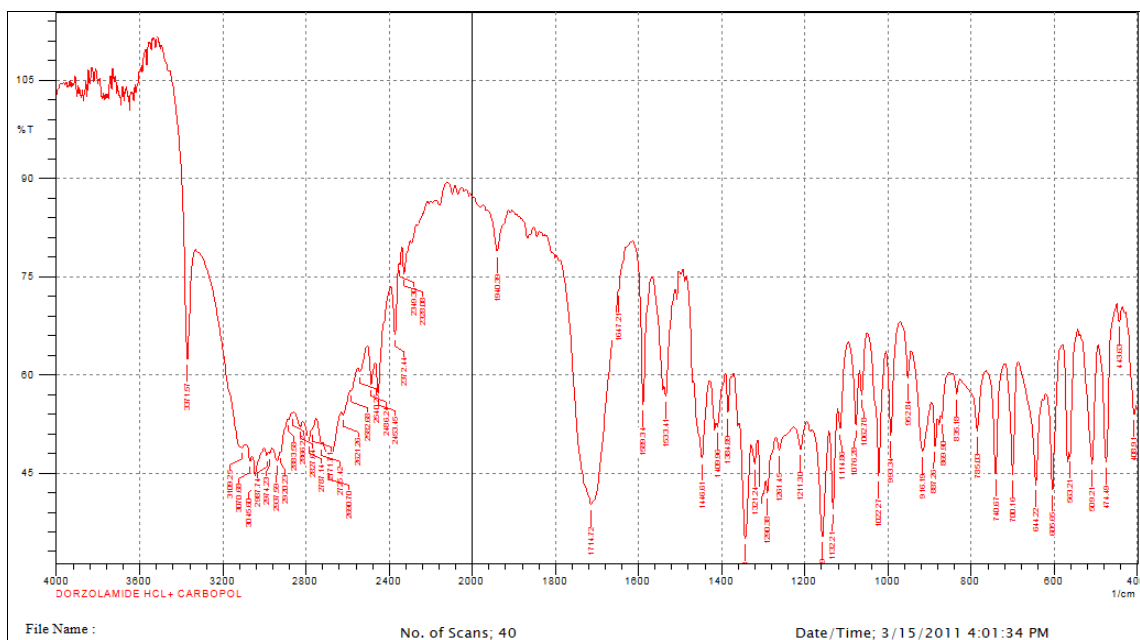
Evaluation for the gelling system was done w.r.t clarity and appearance. The physical appearance of all seven formulations showed that, they all were free flowing liquids and slightly milky in appearance. The milky appearance can be attributed to the polymers present in the formulations. The pH of all sols were very close to

the physiological pH while the gels were completely neutral. Viscosity studies were done using Brookfield Viscometer. Rheological studies The Formulation was shear thinning and an increase in shear stress was observed with increase in angular velocity (pseudo plastic rheology). The drug content uniformity was calculated for all seven formulations, the results of which are tabulated as below. For the various formulations the drug content uniformity varies between 97.62% to 99.33%.

Solid state compatibility studies were carried out on Drug-Polymer mixtures. The study indicates that the peaks in the physical mixture correlate with the drug spectrum ranging from 4000-400 $\text{cm}^{-1}$ . Also there were neither alterations in the major/ characteristic peaks nor the appearance of any extra peaks indicating that the drug is compatible with all the added excipients.



**Fig 2:** Spectra of Dorzolamide Hydrochloride (Pure Drug) Pure drug shows a sharp peak a in the region of infra red.



release from the batches containing lower polymer content was higher than the batches containing higher polymer content (F3, F6). This happened probably because higher concentrations of polymers show higher extent of gelling and hence the drug cannot penetrate the gel matrix and come out in the surrounding dissolution medium. Out of the two polymers used, Xanthan gum has shown the highest and the fastest drug release. The formulation F4 containing 0.2% w/v of Xanthan Gum has shown the drug release of 90.84% and hence this batch is taken as the best batch. The lowest release (78.98%) is shown by formulation F7 which is prepared by using both the polymers in combinations by reducing their concentrations to half. The formulation F2, containing Carbopol 971 P NF has also shown a good release of 88.64%. As expected from Carbopol, it combined with HPMC to give a reasonably sustained drug release. The release data was plotted for Zero Order and First Order kinetics and these plots were subjected to linear regression analysis. The regression coefficients of both the plots were calculated for comparison purposes. Zero Order plots for all the formulations were found to be linear. The regression coefficients predict that the release from the formulations best fit the Zero Order plots. Hence it can be concluded that the all the drug release from all the formulations follow the Zero order kinetics. The drug release data was also plotted for Peppas's model. These plots were also linear and the slope values (n) were more than 0.5 indicating that the drug release is by Non-Fickian diffusion.

Further, to ascertain whether the drug release is also prompted by erosion mechanism, the data was subjected to Erosion Plot. The regression coefficients were calculated which indicate that

the data is best fitted to Erosion Plot for all formulations.

Hence it can be concluded that all the batches showed fairly high drug release because of presence of both diffusion and erosion mechanisms.

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